

MEDICAL IMAGING INFORMATICS:

Lecture # 1

Basics of Medical Imaging Informatics:

Estimation Theory

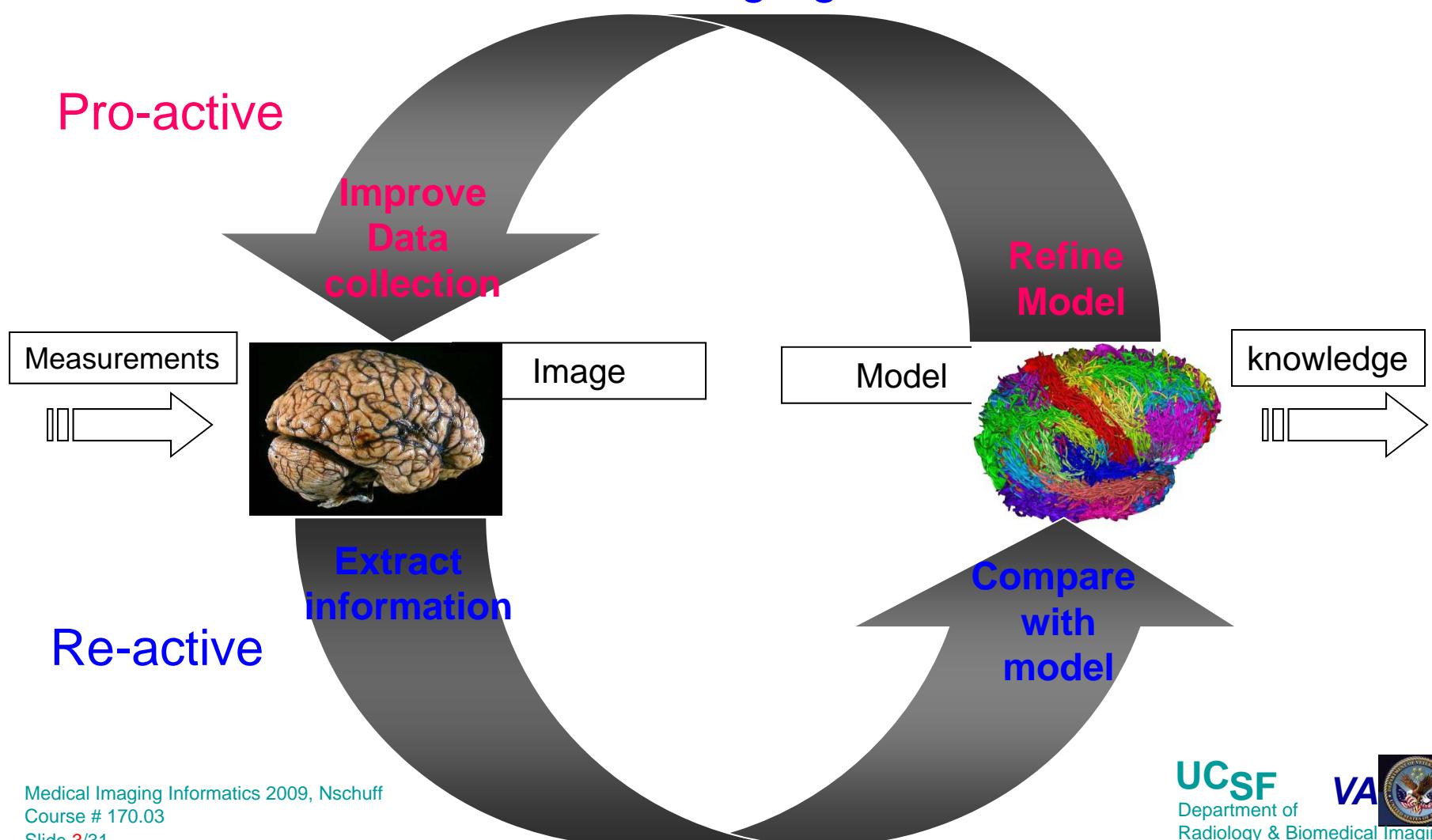
Norbert Schuff
Professor of Radiology
VA Medical Center and UCSF
Norbert.schuff@ucsf.edu

What Is Medical Imaging Informatics?

- Signal Processing
 - [Digital Image Acquisition](#)
 - [Image Processing and Enhancement](#)
- Data Mining
 - [Computational anatomy](#)
 - [Statistics](#)
 - [Databases](#)
 - [Data-mining](#)
 - Workflow and Process Modeling and Simulation
- Data Management
 - Picture Archiving and Communication System (PACS)
 - Imaging Informatics for the Enterprise
 - Image-Enabled Electronic Medical Records
 - Radiology Information Systems (RIS) and Hospital Information Systems (HIS)
 - Quality Assurance
 - Archive Integrity and Security
- Data Visualization
 - Image Data Compression
 - 3D, Visualization and Multi-media
 - DICOM, HL7 and other Standards
- Teleradiology
 - Imaging Vocabularies and Ontologies
 - Transforming the Radiological Interpretation Process (TRIP)[\[2\]](#)
 - Computer-Aided Detection and Diagnosis (CAD).
 - Radiology Informatics Education
- Etc.

What Is The Focus Of This Course?

Learn using computational tools to maximize information for knowledge gain:



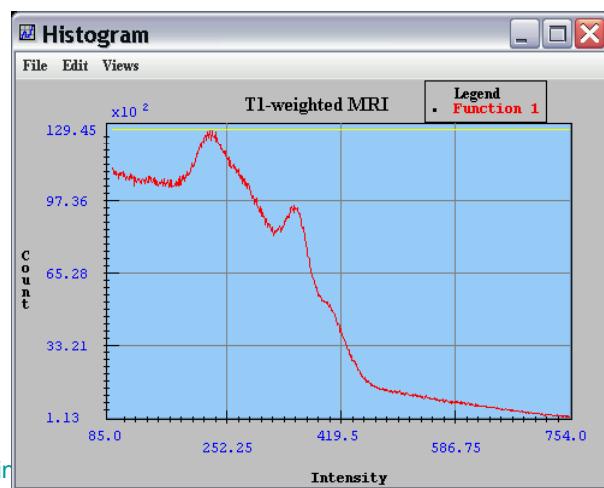
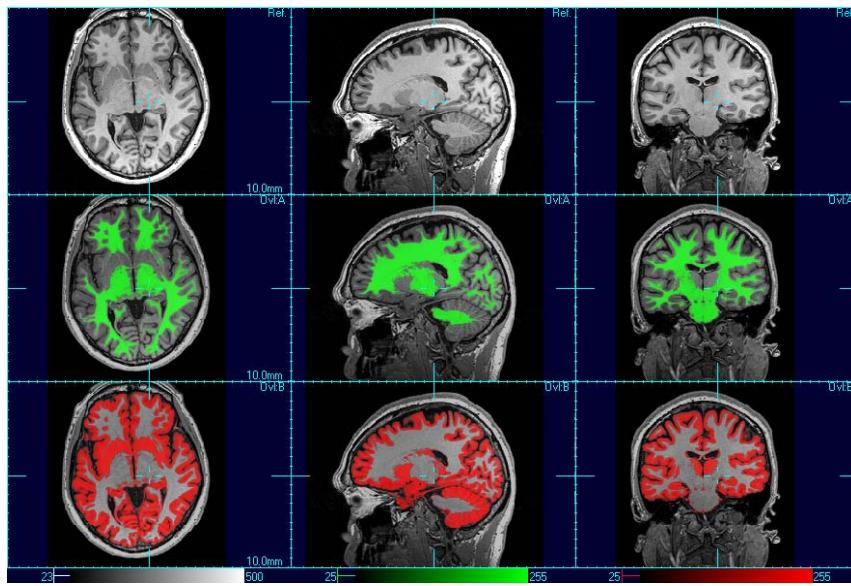
Challenge: Maximize Information Gain

1. Q: How can we estimate quantities of interest from a given set of uncertain (noise) measurements?
A: *Apply estimation theory* (1st lecture today)

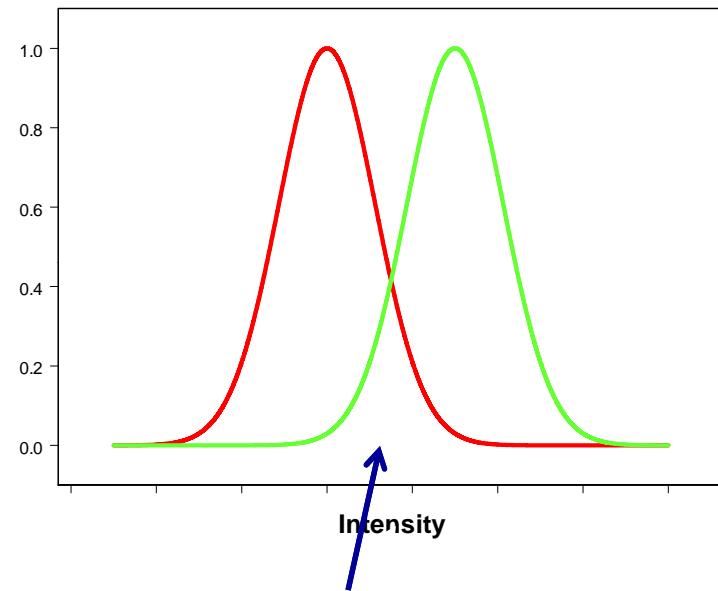
2. Q: How can we measure (quantify) information?
A: *Apply information theory* (2nd lecture next week)

Estimation Theory: Motivation Example I

Gray/White Matter Segmentation



Hypothetical Histogram



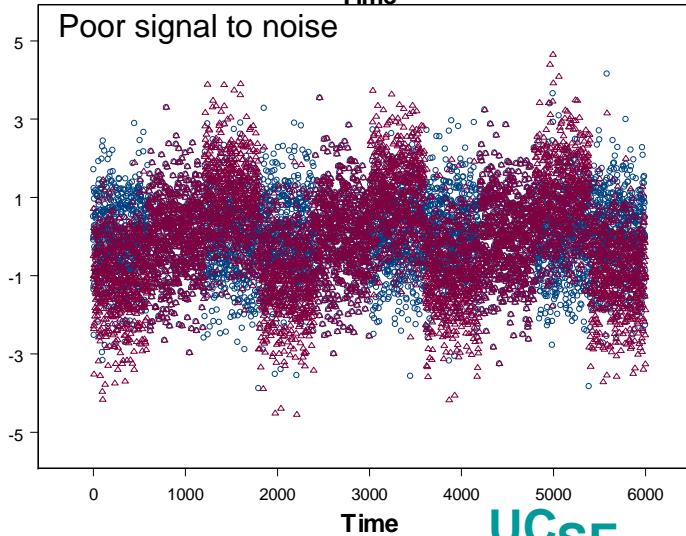
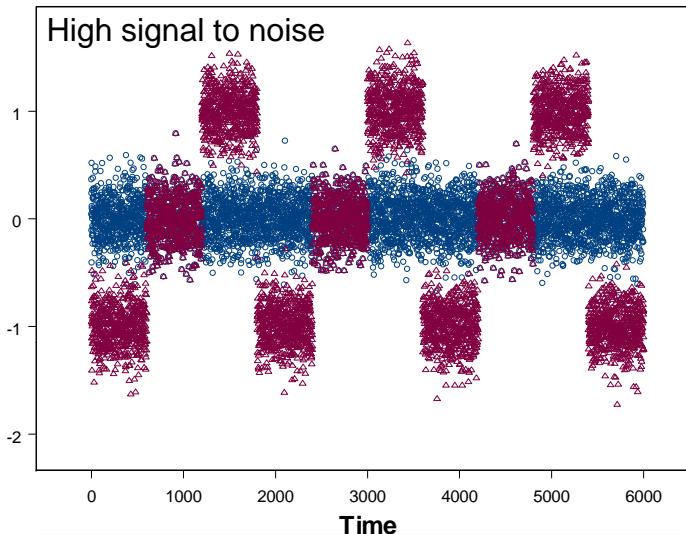
GM/WM overlap 50:50;
Can we do better than flipping a coin?

Estimation Theory: Motivation Example II

Goal: Capture dynamic signal on a static background



D. Feinberg Advanced MRI Technologies, Sebastopol, CA

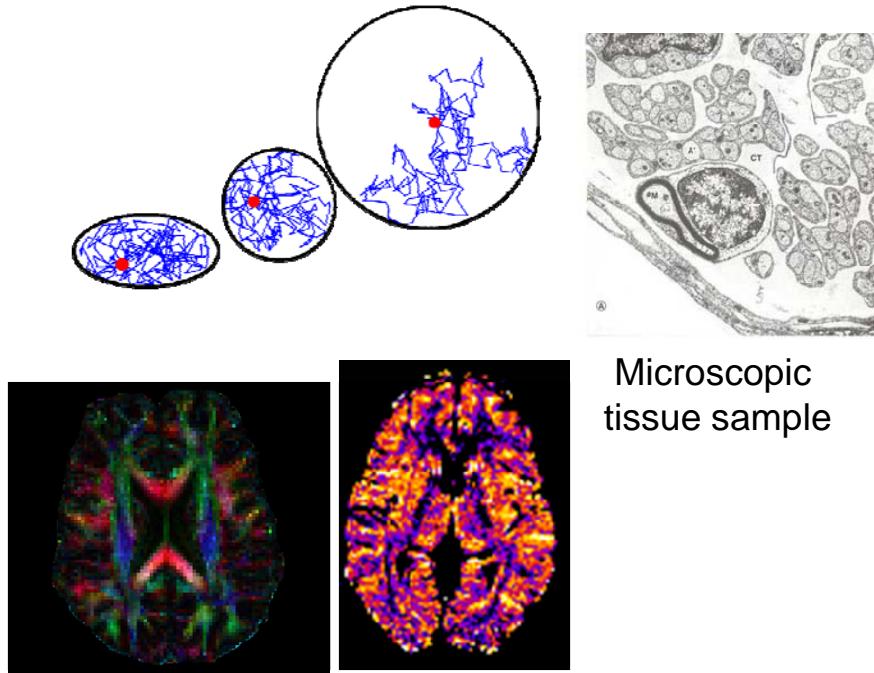


Estimation Theory: Motivation Example III

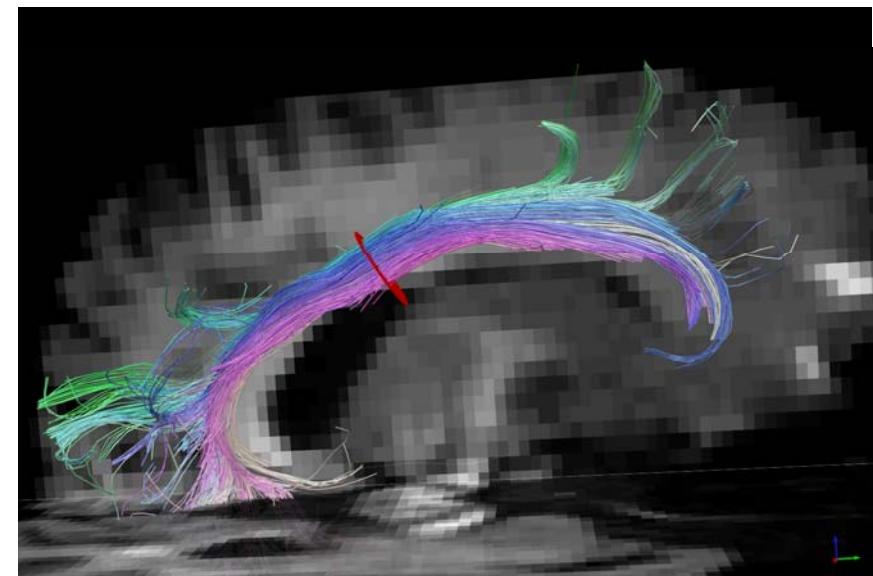
Diffusion Imaging

- Sensitive to random motion of water
- Probes structures on a microscopic scale

Goal:
Capture directions
of fiber bundles



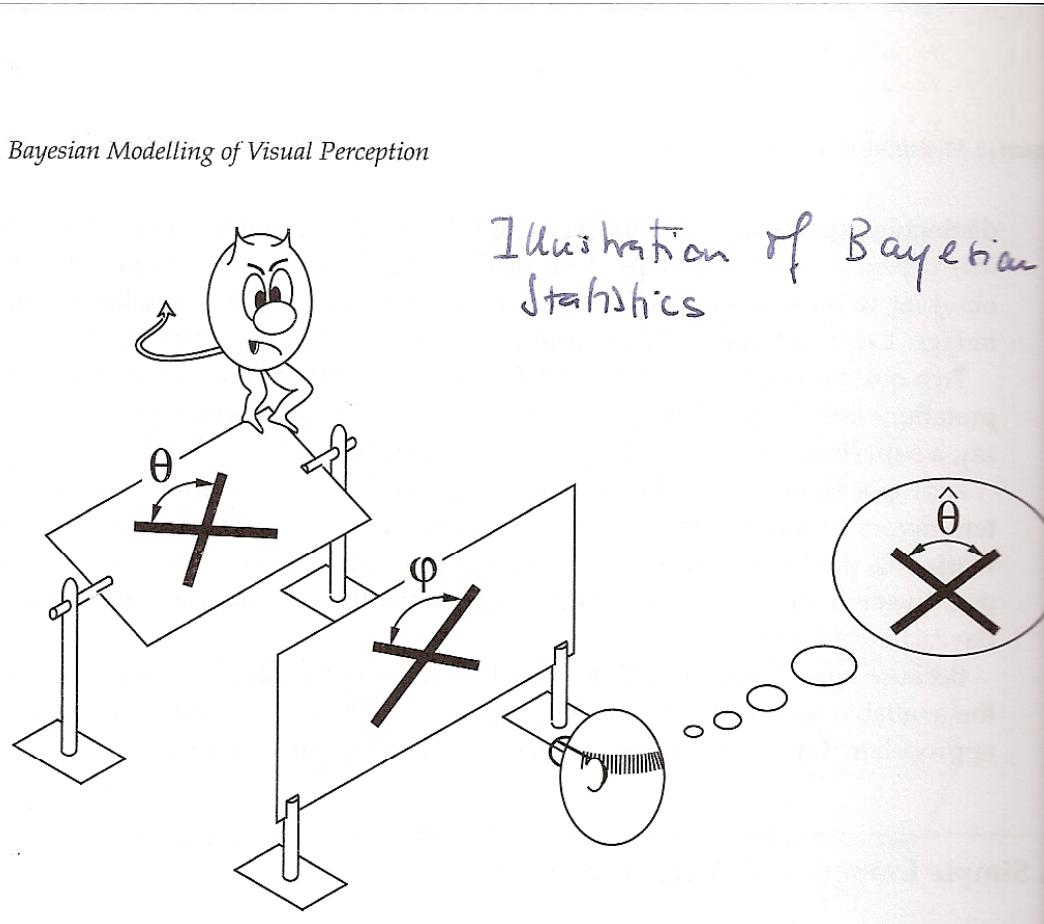
Quantitative Diffusion Maps



Dr. Van Wedeen, MGH

Basic Concepts of Modeling

16 Bayesian Modelling of Visual Perception



Θ : target of interest
and unknown

ρ : measurement

$\hat{\Theta}$: Estimator - a good
guess of Θ based on
measurements

Cartoon adapted from: [Rajesh P. N. Rao, Bruno A. Olshausen](#) Probabilistic Models of the Brain.
MIT Press 2002.

Deterministic Model

16 Bayesian Modelling of Visual Perception

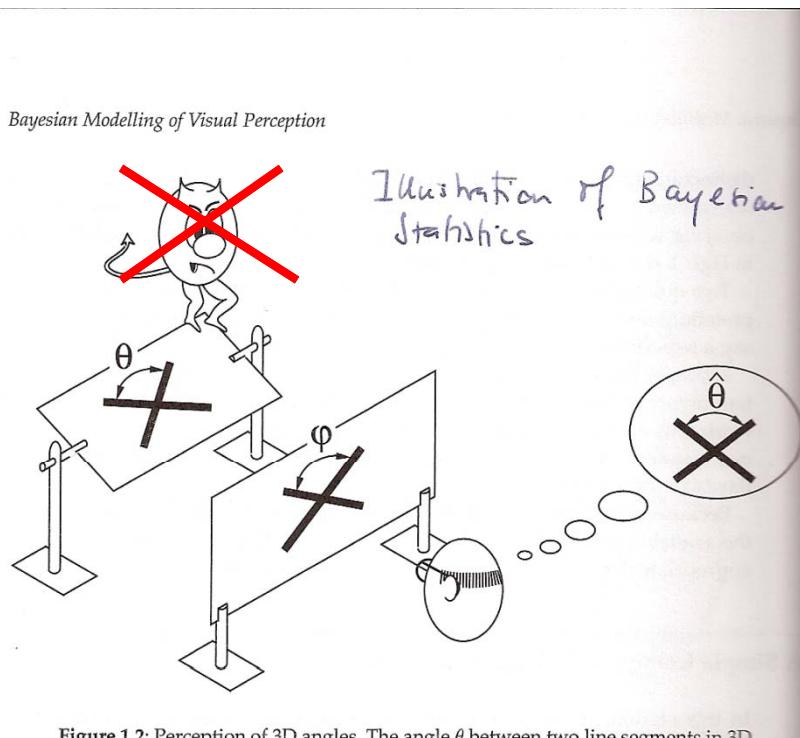


Figure 1.2: Perception of 3D angles. The angle θ between two line segments in 3D

N = number of measurements

M = number of states, M=1 is possible

Usually N > M and $|\text{noise}|^2 > 0$

$$\varphi_N = H\theta_M + \text{noise}_N$$

The model is deterministic, because discrete values of Θ are solutions.

Note:

- 1) we make no assumption about Θ
- 2) Each value is as likely as any another value

What is the best estimator under these circumstances?

Least-Squares Estimator (LSE)

The best what we can do is minimizing noise:

$$\varphi_N - H\theta_M = noise_M$$

$$\varphi_N - H\hat{\theta}_{LSE} = 0$$

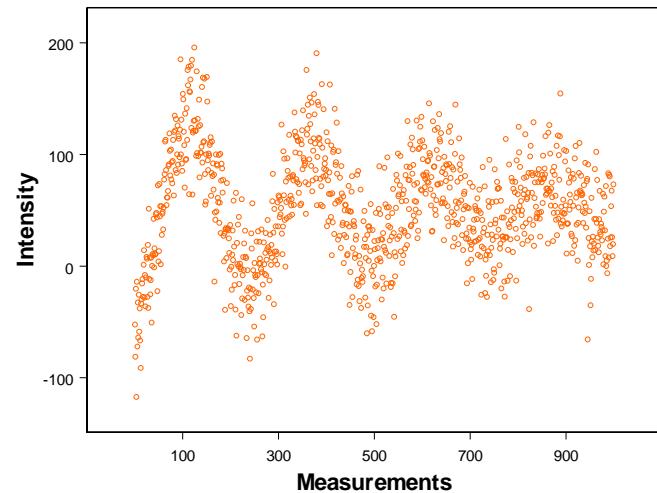
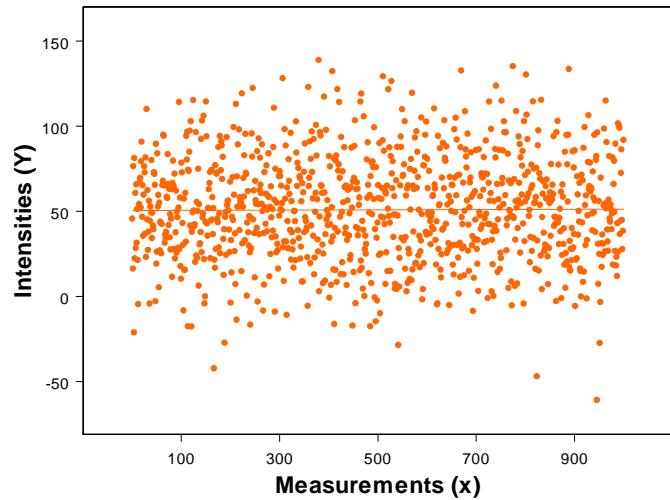
$$H^T \varphi_N - (H^T H) \hat{\theta}_{LSE} = 0$$

$$\hat{\theta}_{LSE} = (H^T H)^{-1} H^T \varphi_n$$

- LSE is popular choice for model fitting
 - Useful for obtaining a descriptive measure
- But
- LSE makes no assumptions about distributions of data or parameters
 - Has no basis for statistics → “deterministic model”



Prominent Examples of LSE



Mean Value: $\hat{\theta}_{mean} = \frac{1}{N} \sum_{j=1}^N \varphi(j)$

Variance $\hat{\theta}_{variance} = \frac{1}{N-1} \sum_{j=1}^N (\varphi(j) - \hat{\theta}_{mean})^2$

Amplitude $\hat{\theta}_1$

Frequency $\hat{\theta}_2$

Phase $\hat{\theta}_3$

Decay $\hat{\theta}_4$

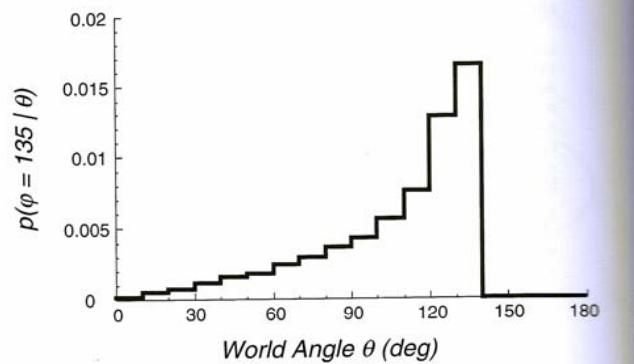


Likelihood Model

Likelihood

$$L_\varphi(\Phi) = p(\varphi | \Phi)$$

18 Bayesian Modelling of Visual Perception



16 Bayesian Modelling of visual perception

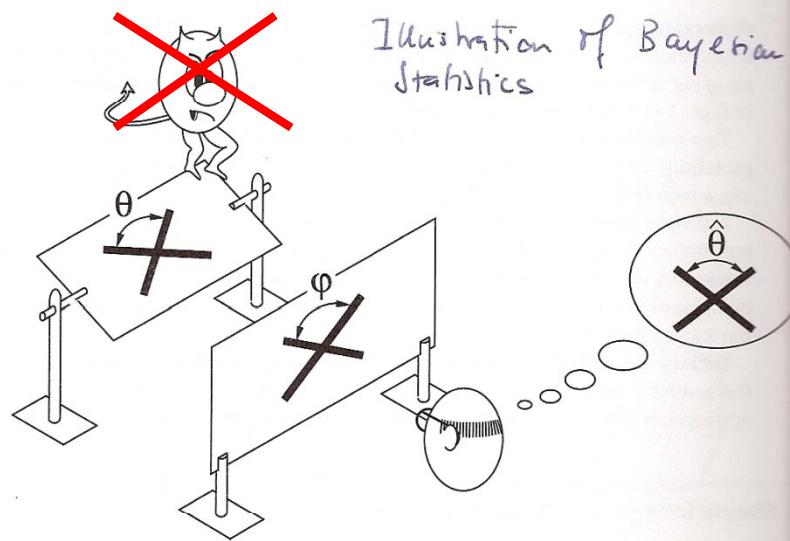


Figure 1.2: Perception of 3D angles. The angle θ between two line segments in 3D

Pretend we know something about Θ

We perform measurements for all possible values of Θ

We obtain the likelihood function of Θ given our measurements ρ

Note:

Θ is random

φ is a fixed parameter

Likelihood is a function of both the unknown Θ and known φ



Likelihood Model (cont'd)

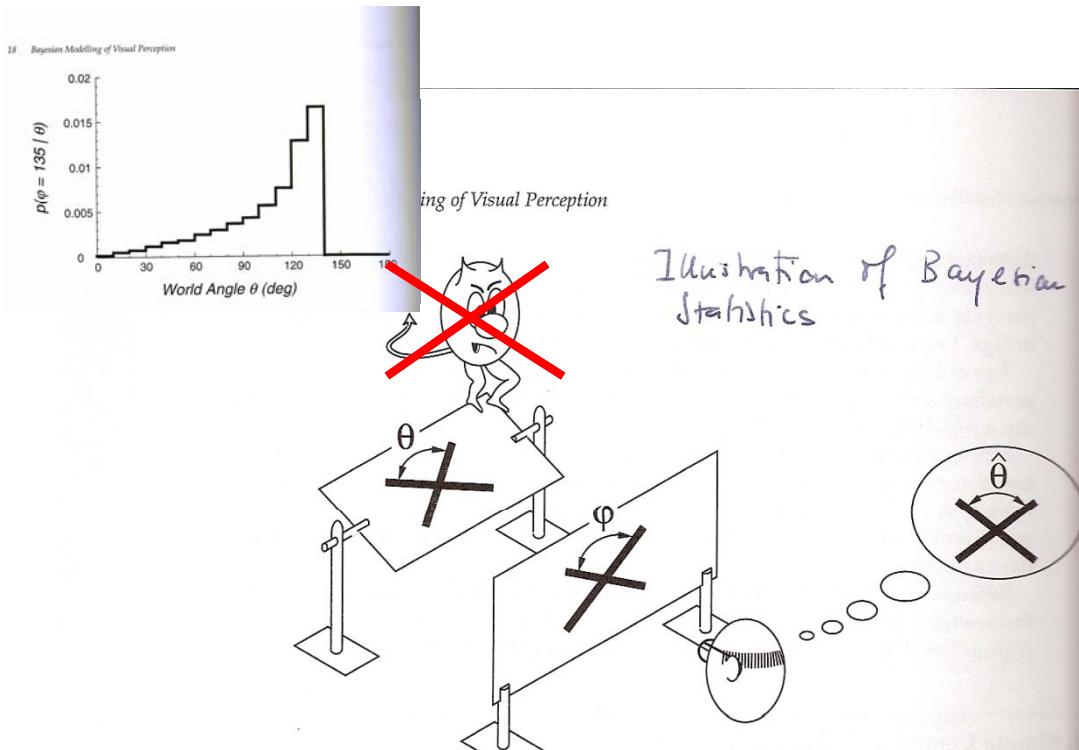


Figure 1.2: Perception of 3D angles. The angle θ between two line segments in 3D

$$L_\varphi(\Theta) = p(\varphi_N | \Theta)$$

New Goal:
Find an estimator
which gives the most likely
probability distribution
underlying $L_\varphi(\Theta)$

Maximum Likelihood Estimator (MLE)

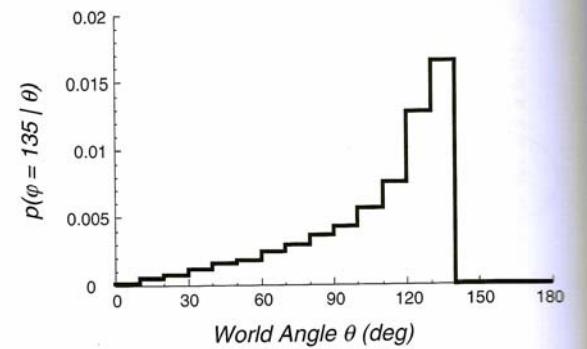
Goal: Find estimator which gives the most likely probability distribution underlying \mathbf{x}_N .

$$\hat{\Theta}_{MLE} = \max_{\Theta} p(\varphi_N | \Theta) \quad \text{Max likelihood function}$$

Θ_{MLE} can be found by taking the derivative of Likelihood F

$$\frac{d}{d\Theta} \ln p(\varphi_N | \Theta) \Big|_{\Theta=\Theta_{MLE}} = 0$$

18 Bayesian Modelling of Visual Perception



Example I: MLE Of Normal Distribution

Normal distribution

$$p(\varphi_N | \bar{\Theta}, \sigma^2) = \exp \left[\frac{1}{2\sigma^2} \sum_{j=1}^N (\varphi(j) - \bar{\Theta})^2 \right]$$

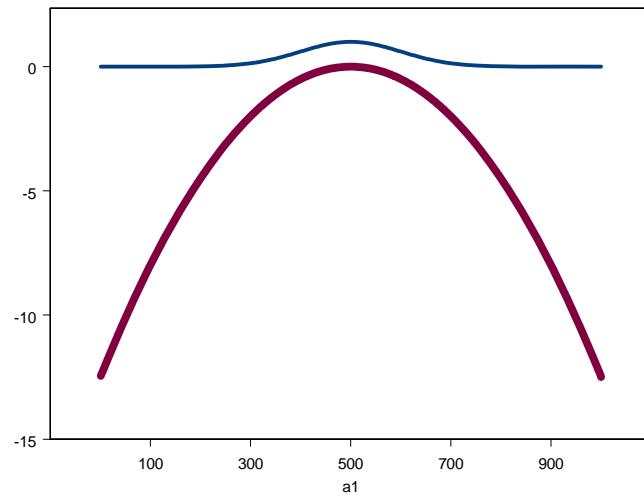
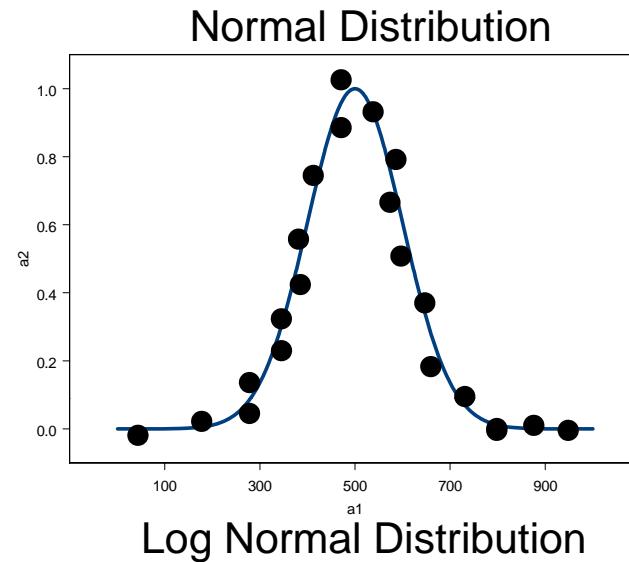
log of the normal distribution (normD)

$$\ln p(\varphi_N | \bar{\Theta}, \sigma^2) = \frac{1}{2\sigma^2} \sum_{j=1}^N (\varphi(j) - \bar{\Theta})^2$$

MLE of the mean (1st derivative):

$$\frac{d}{d\hat{\Theta}_{MLE}} \ln p(\square) = \frac{1}{4\hat{\sigma}^2} \sum_{j=1}^N (\varphi(j) - \hat{\Theta}_{MLE}) = 0$$

$$\hat{\Theta}_{MLE} = \frac{1}{N} \sum_{j=1}^N \varphi(j)$$

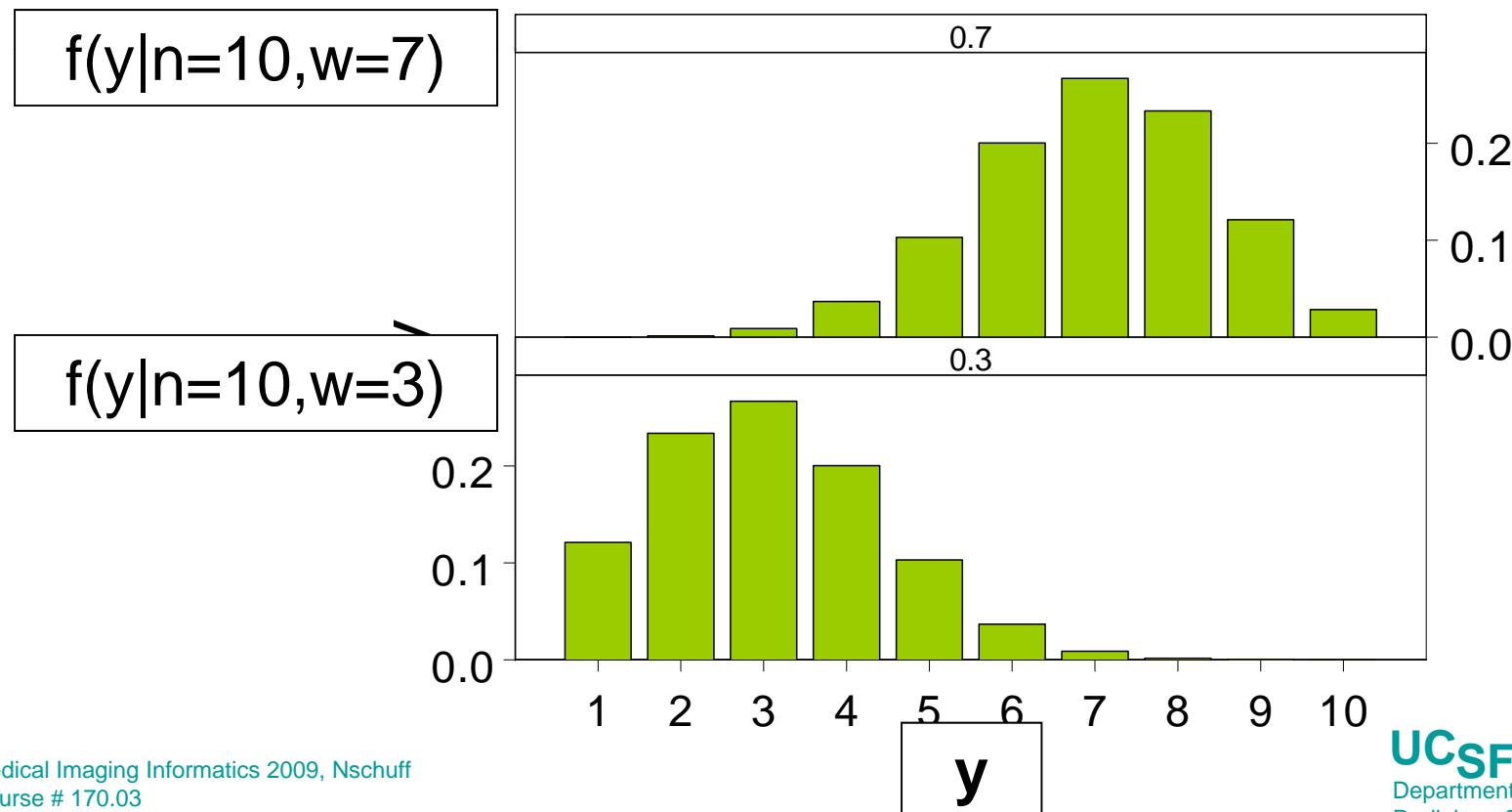


Example II: MLE Of Binomial Distribution (Coin Toss)

Distribution function $f(y|n,w)$:

n = number of tosses

w = probability of success



MLE Of Coin Toss (cont'd)

Goal:

Given the observed data $f(y|w=0.7, n=10)$, find the parameter Θ_{MLE} that most likely produced the data.

$$L(\Theta_{MLE} \mid y = 7, n = 10)$$

For a fair coin $\Theta_{MLE} = 0.5$

MLE Of Coin Toss (cont'd)

Likelihood function of coin tosses

$$L(\Phi | y) = \frac{n!}{(y!)(n-y)!} \cdot \Phi^y (1-\Phi)^{n-y}$$

What is the likelihood of observing 7 heads given that we tossed a fair coin 10 times

$$L(\Theta | n=10, w=7) = \frac{10!}{(7!)(10-7)!} \cdot 0.5^7 (1-0.5)^{10-7} = 0.12$$

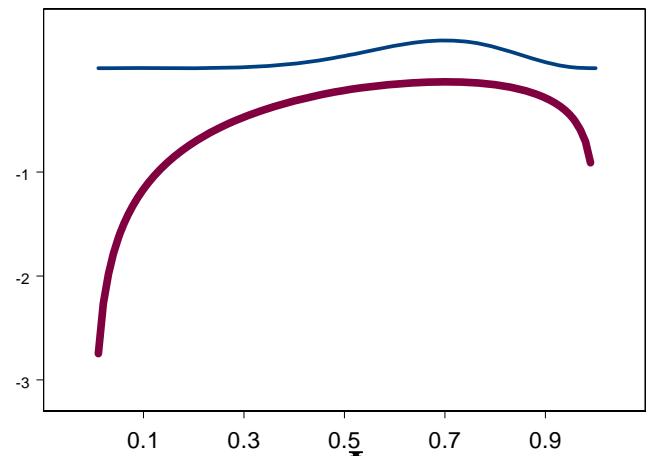
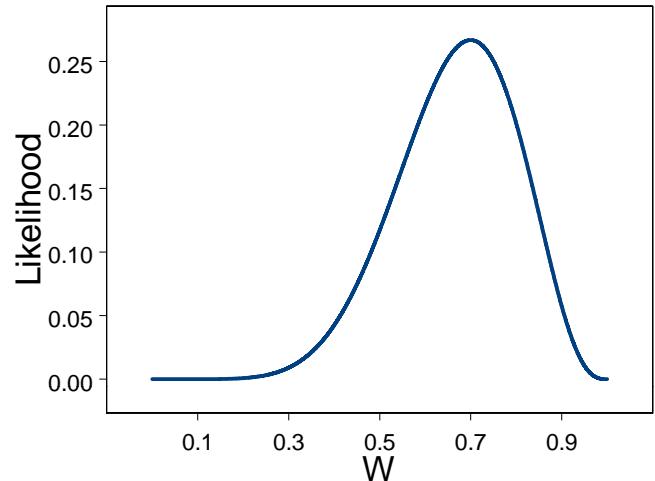
unfair coin $\Theta=0.6$

$$L(\Theta | n=10, w=7) = \frac{10!}{(7!)(10-7)!} \cdot 0.6^7 (1-0.6)^{10-7} = 0.21$$

log likelihood function

$$\ln L(w | y) =$$

$$\ln \frac{n!}{(y!)(n-y)!} + y \ln w + (n-y) \ln (1-w)$$



MLE Of Coin Toss

Evaluate MLE equation (1st derivative)

$$\frac{d \ln L(\Phi)}{d \Phi_{MLE}} = \frac{y}{\Phi_{MLE}} - \frac{(n-y)}{1-\Phi_{MLE}} = 0$$

$$= \frac{y - n\Phi_{MLE}}{\Phi_{MLE}(1-\Phi_{MLE})} = 0 \Rightarrow \Phi_{MLE} = \frac{y}{n}$$

According to the MLE principle, the distribution $f(y/n)$ for a given n is the most likely distribution to have generated the observed data of y .

Relationship between MLE and LSE

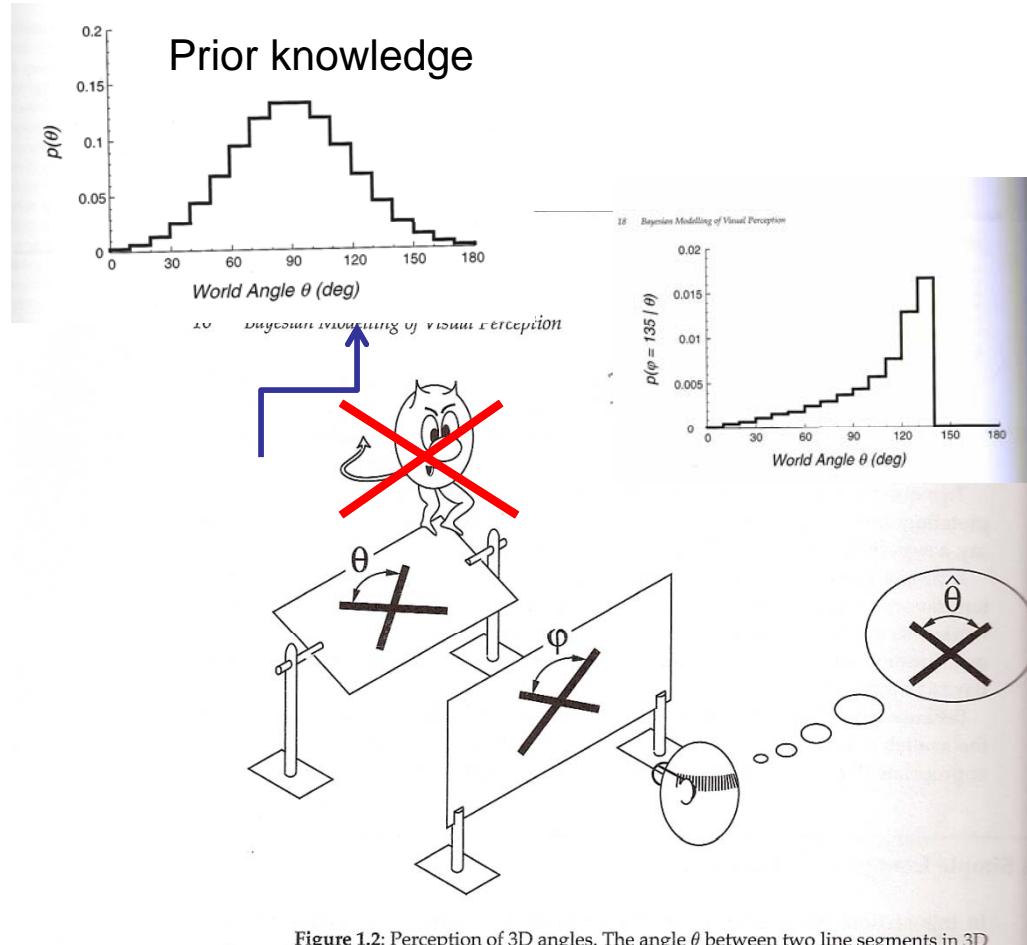
Assume: Θ is independent of noise_N
MLE and noise_N have the same distribution

$$p_{\theta}(\varphi_N | \Theta) = p_{noise}(\varphi_N - H\Theta | \Theta)$$

noise_N is zero mean and gaussian

p($\rho | \Theta$) is maximized when LSE is minimized

Bayesian Model



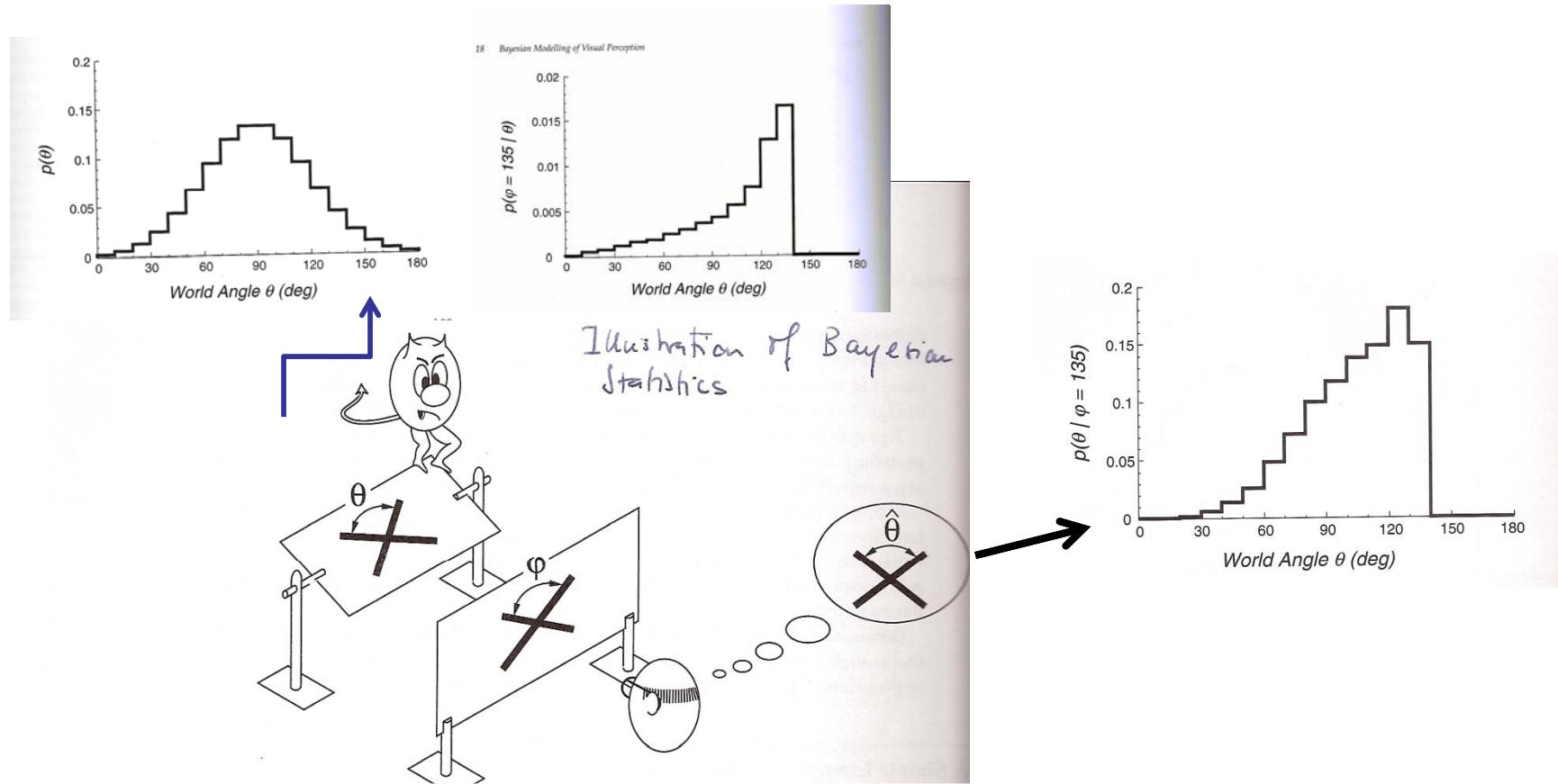
Now, the daemon comes into play, but we know The daemon's preferences for Θ (prior knowledge).

$$prior(\Theta) = p(\Theta)$$

New Goal:
Find the estimator which gives the most likely probability distribution of Θ given everything we know.



Bayesian Model



$$posterior_{\varphi}(\Theta) = C \cdot L_{\varphi}(\varphi_N | \Theta) \cdot p(\Theta)$$

Maximum A-Posteriori (MAP) Estimator

Goal:

Find the most likely Θ_{MAP} (max. posterior density of φ) given φ .

$$\widehat{\Theta}_{MAP} = \max L(\varphi_N | \Theta) p(\varphi_N)$$

Maximize joint density

Θ_{MAP} can be found by taken the partial derivative

$$\frac{d}{d\Theta} \ln L(\varphi_N | \Theta) p(\varphi_N) = \frac{\partial}{\partial \Theta} \ln L(\varphi_N | \Theta) + \frac{\partial}{\partial \Theta} \ln p(\varphi_N) = 0$$

Example III: MAP Of Normal Distribution

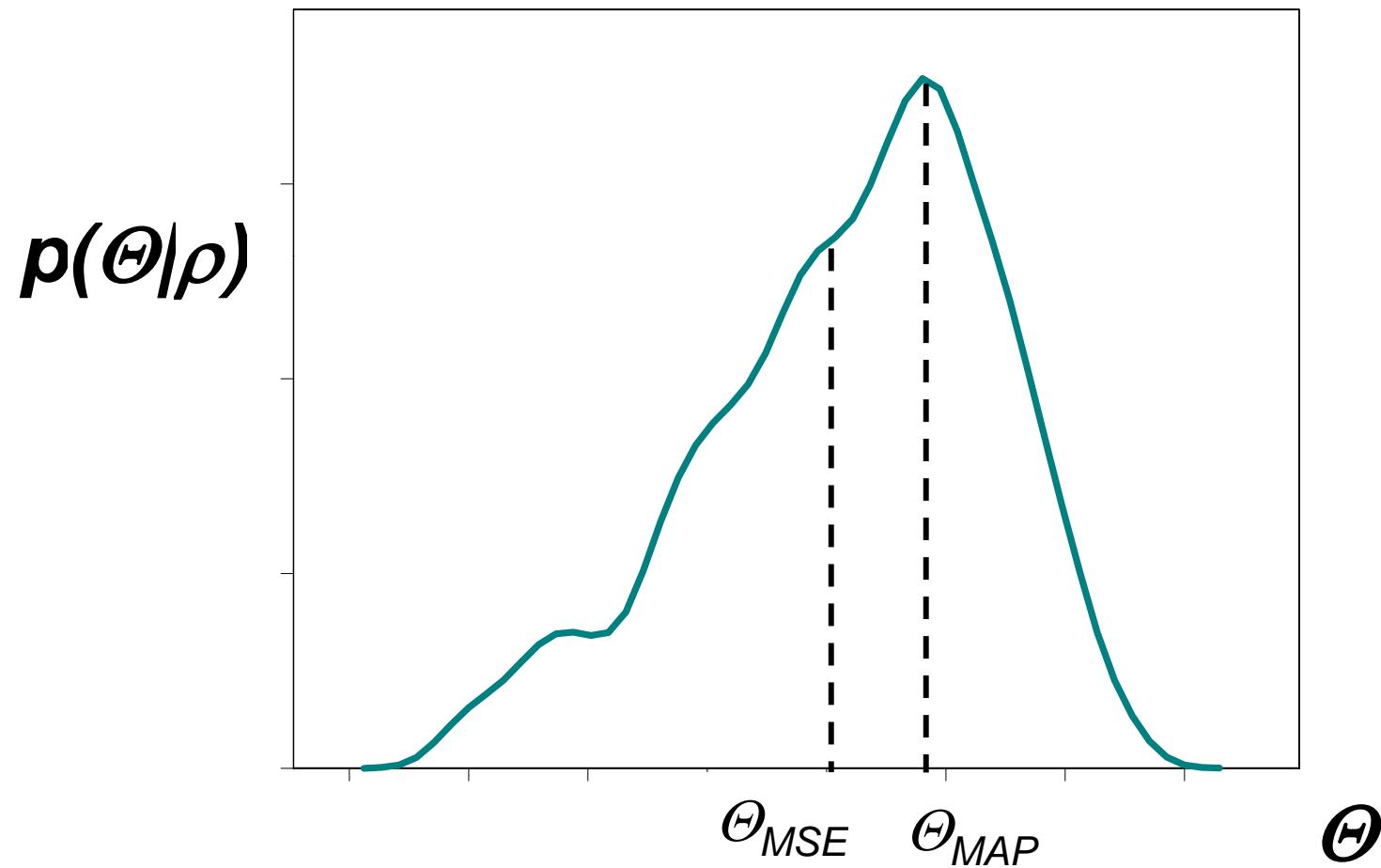
The sample mean of MAP is:

$$\hat{\Phi}_{\text{MAP}} = \frac{\sigma_\mu^2}{\sigma_\phi^2 + T\sigma_\mu^2} \sum_{j=1}^N \varphi(j)$$

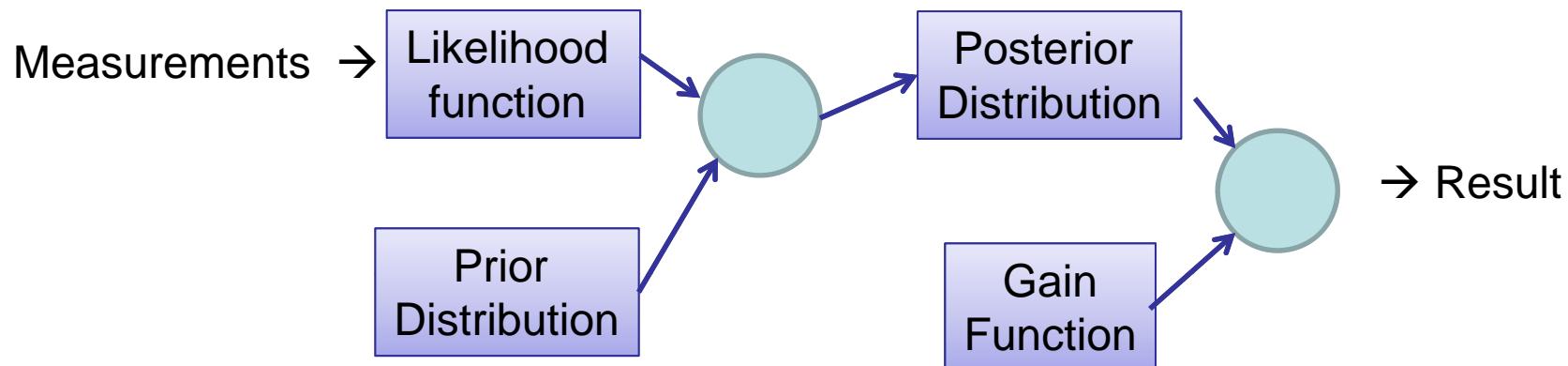
If we do not have prior information on μ , $\sigma_\mu \rightarrow \inf$ or $T \rightarrow \inf$

$$\hat{\mu}_{\text{MAP}} \Rightarrow \hat{\mu}_{\text{ML}}, \hat{\mu}_{\text{LSE}}$$

Posterior Distribution and Decision Rules



Decision Rules



Some Desirable Properties of Estimators I:

Unbiased: Mean value of the error should be zero

$$E\langle \hat{\Phi} - \Phi \rangle = 0$$

Consistent: Error estimator should decrease asymptotically as number of measurements increase. (Mean Square Error (MSE))

$$MSE = E\langle \|\hat{\Phi} - \Phi\|^2 \rangle \rightarrow 0 \text{ for large } N$$

What happens to MSE when estimator is biased?

$$MSE = E\langle \|\hat{\Phi} - \Phi - b\|^2 \rangle + E\langle \|b\|^2 \rangle$$

variance

bias



Some Desirable Properties of Estimators II:

Efficient: Co-variance matrix of error should decrease asymptotically to its minimal value for large N

$$C_{\tilde{\theta}} = E \left\langle (\hat{\Phi}_i - \Phi_i)(\hat{\Phi}_k - \Phi_k)^T \right\rangle \leq \text{some.very.small.value}$$

Example: Properties Of Estimators Mean and Variance

Mean:
$$E\langle \hat{\mu} \rangle = \frac{1}{N} \sum_{j=1}^N E\langle \varphi(j) \rangle = \frac{1}{N} \cdot N\mu = \mu$$

The sample mean is an unbiased estimator of the true mean

Variance:
$$E\langle (\hat{\mu} - \mu)^2 \rangle = \frac{1}{N^2} \sum_{j=1}^N E\langle (\varphi(j) - \mu)^2 \rangle = \frac{1}{N^2} \cdot N\sigma^2 = \frac{\sigma^2}{N}$$

The variance is a consistent estimator because
It approaches zero for large number of measurements

Properties Of MLE

- **is consistent:** the MLE recovers asymptotically the true parameter values that generated the data for $N \rightarrow \infty$;
- **Is efficient:** The MLE achieves asymptotically the minimum error (= max. information)

Summary

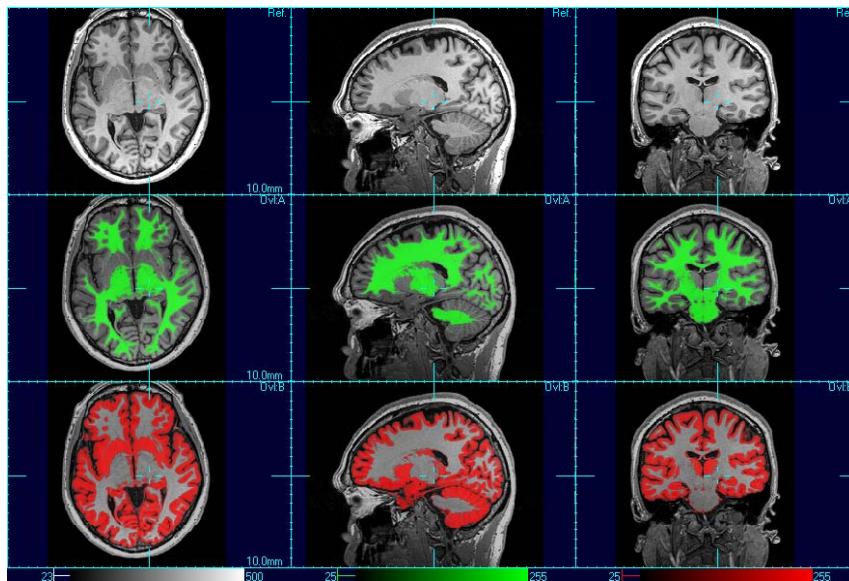
- LSE is a descriptive method to accurately fit data to a model.
- MLE is a method to seek the probability distribution that makes the observed data most likely.
- MAP is a method to seek the most probably parameter value given prior information about the parameters and the observed data.
- If the influence of prior information decreases, i.e. many measurements, MAP approaches MLE

Some Priors in Imaging

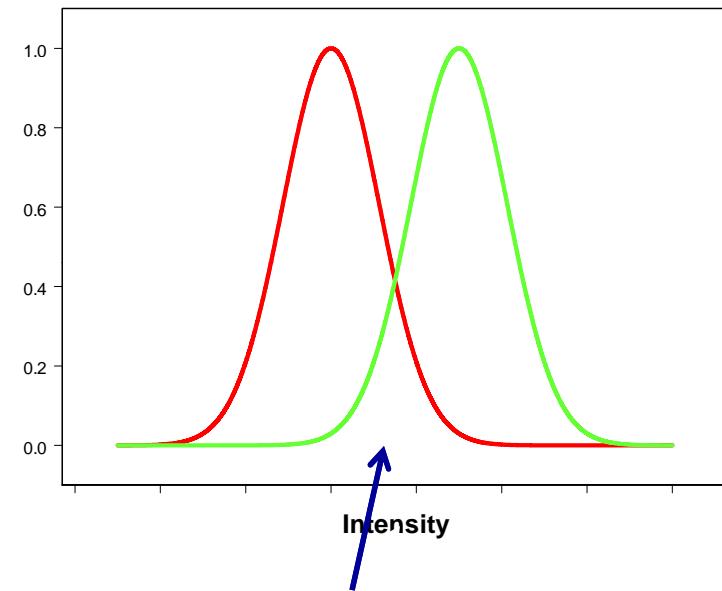
- Smoothness of the brain
- Anatomical boundaries
- Intensity distributions
- Anatomical shapes
- Physical models
 - Point spread function
 - Bandwidth limits
- Etc.

Estimation Theory: Motivation Example I

Gray/White Matter Segmentation



Hypothetical Histogram



What works better than flipping a coin?

Design likelihood functions based on
anatomy
co-occurrence of signal intensities
others

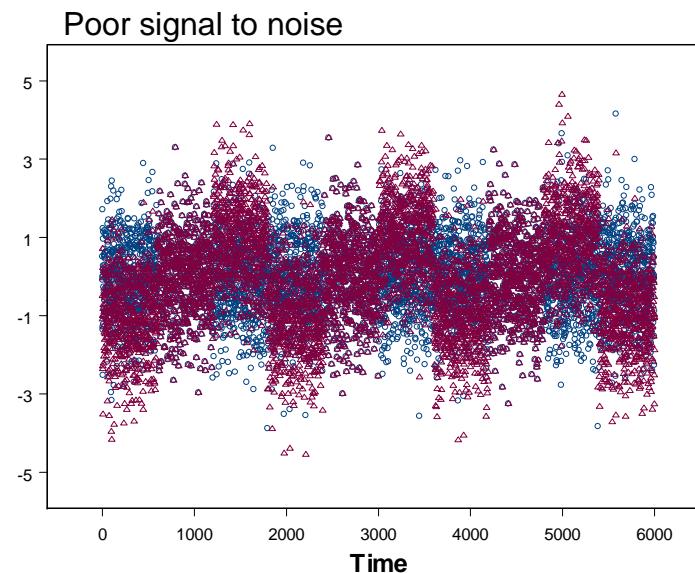
Determine prior distribution
population based atlas of regional intensities
model based distributions of intensities
others

Estimation Theory: Motivation Example II

Goal: Capture dynamic signal on a static background



D. Feinberg Advanced MRI Technologies, Sebastopol, CA



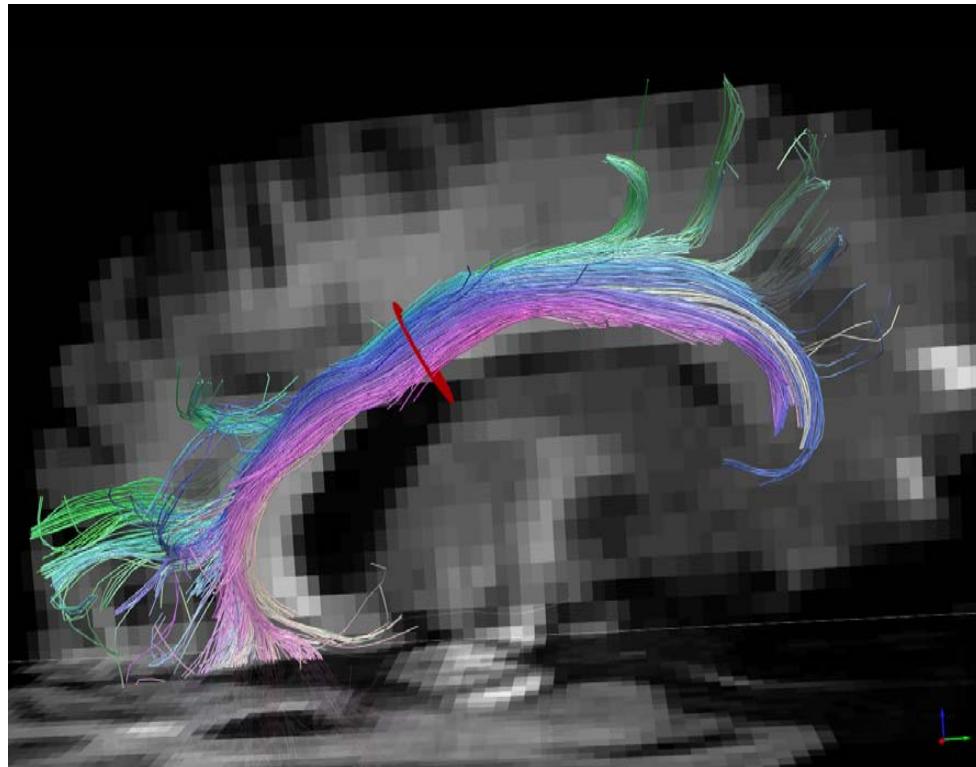
Improvements to identify the dynamic signal:

Design likelihood functions based on
auto-correlations
anatomical information

Determine prior distributions from
serial measurements
multiple subjects
anatomy

Estimation Theory: Motivation Example III

Diffusion Spectrum Imaging – Human Cingulum Bundle



Dr. Van Wedeen, MGH

Goal:
Capture directions
of fiber bundles

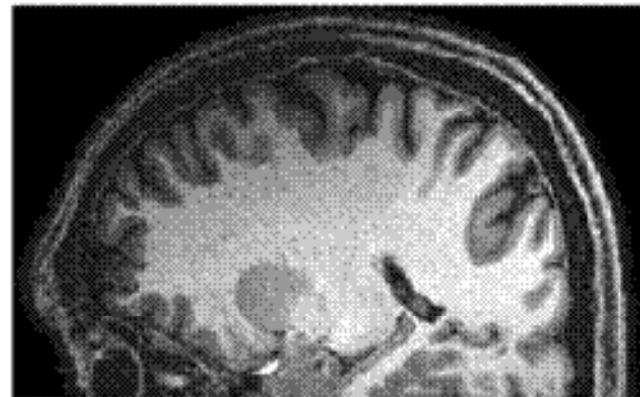
Improvements to identify tracts:

Design likelihood functions based on
similarity measures of adjacent
voxels
fiber anatomy

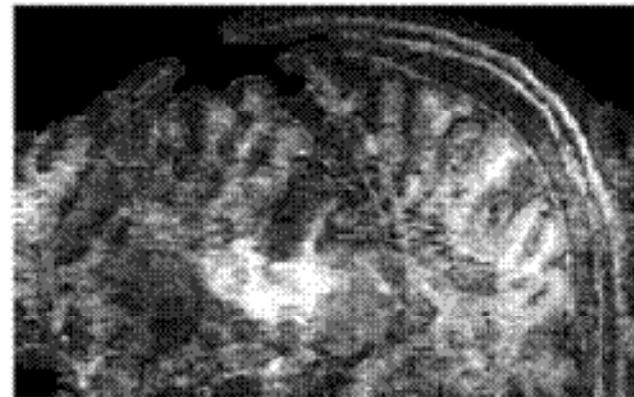
Determine prior distributions from
anatomy
fiber skeletons from a population
others



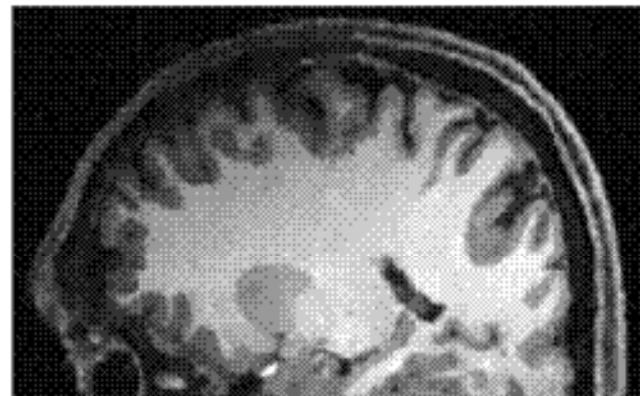
MAP Estimation in Image Reconstructions with Edge-Preserving Priors



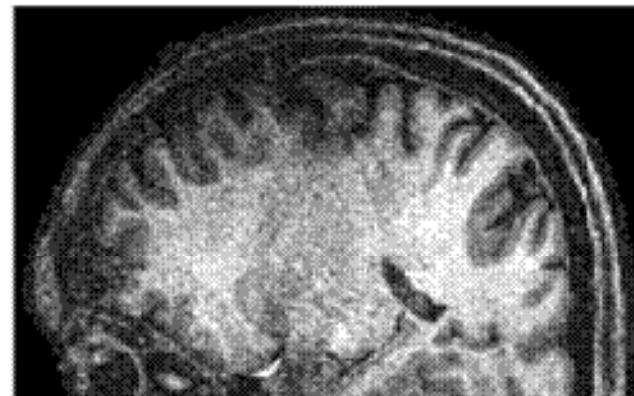
(a)



(c)



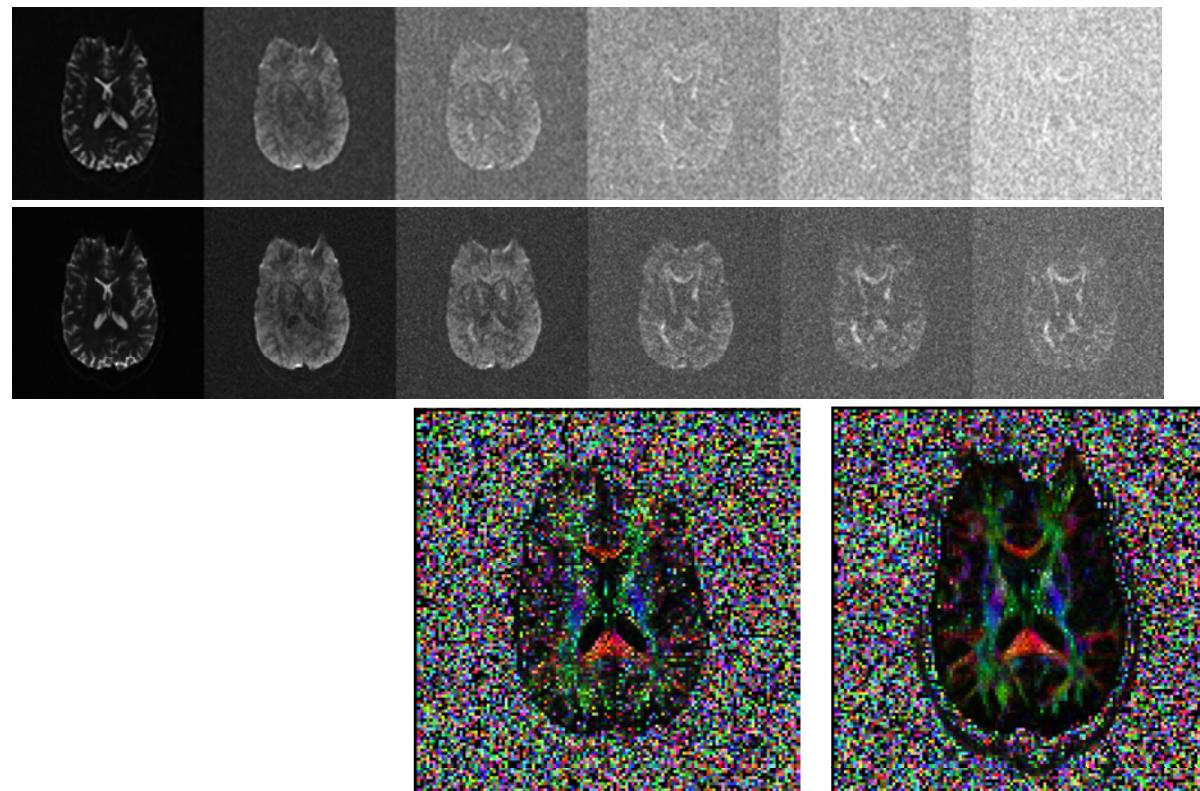
(b)



(d)

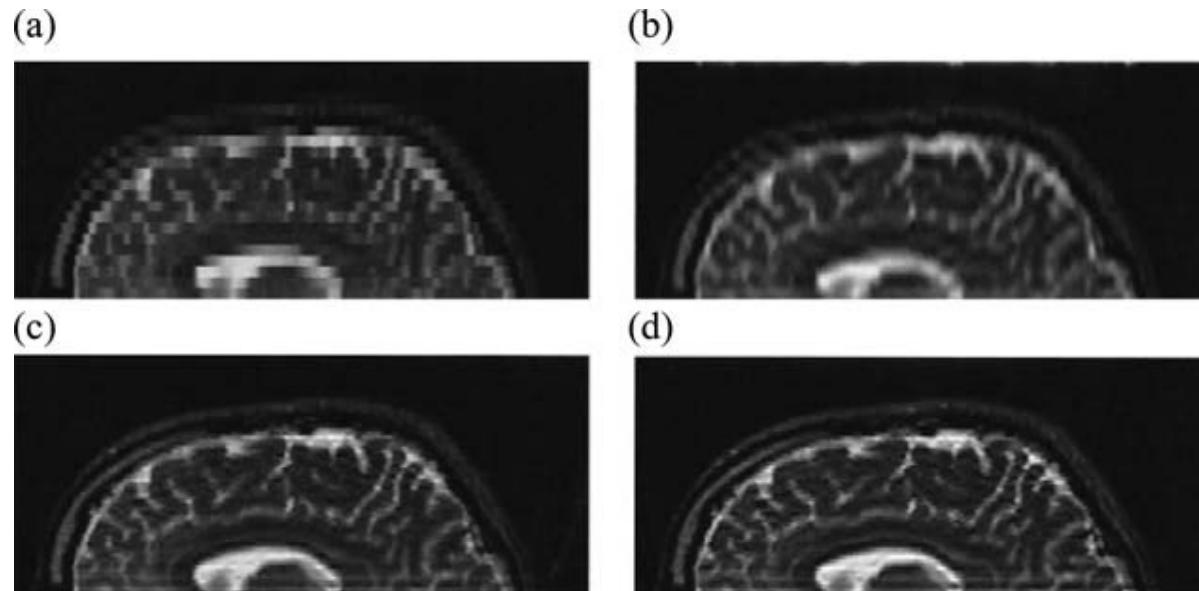
MAP in Image Reconstructions with Edge-Preserving Priors

For DTI, use the fact that coregistered DTI images have common edge features:



Dr. Justin Haldar Urbana-Champaign

MAP Estimation In Image Reconstruction

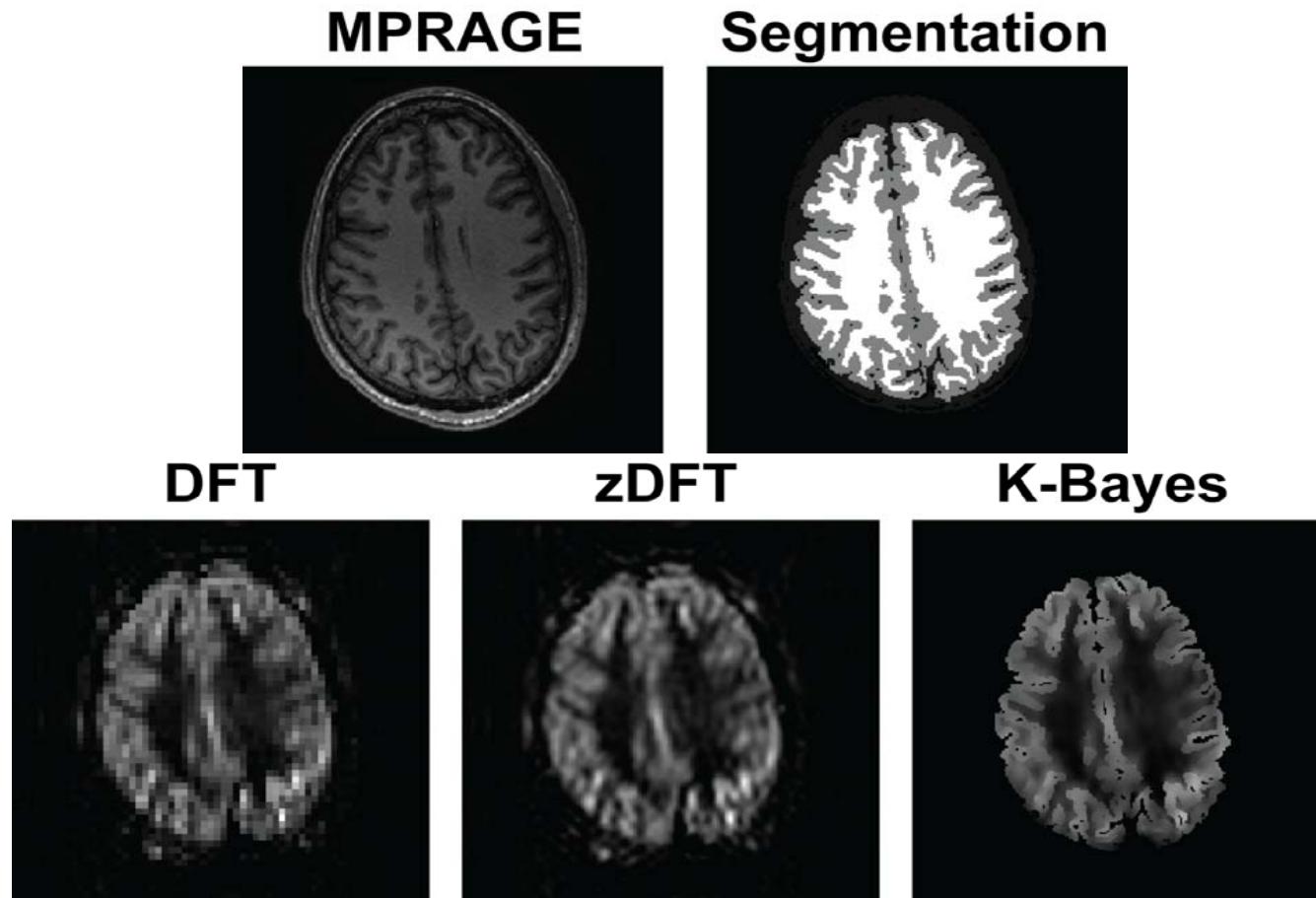


Human brain MRI. (a) The original LR data. (b) Zero-padding interpolation. (c) SR with box-PSF. (d) SR with Gaussian-PSF

From: A. Greenspan in
The Computer Journal Advance Access published February 19, 2008



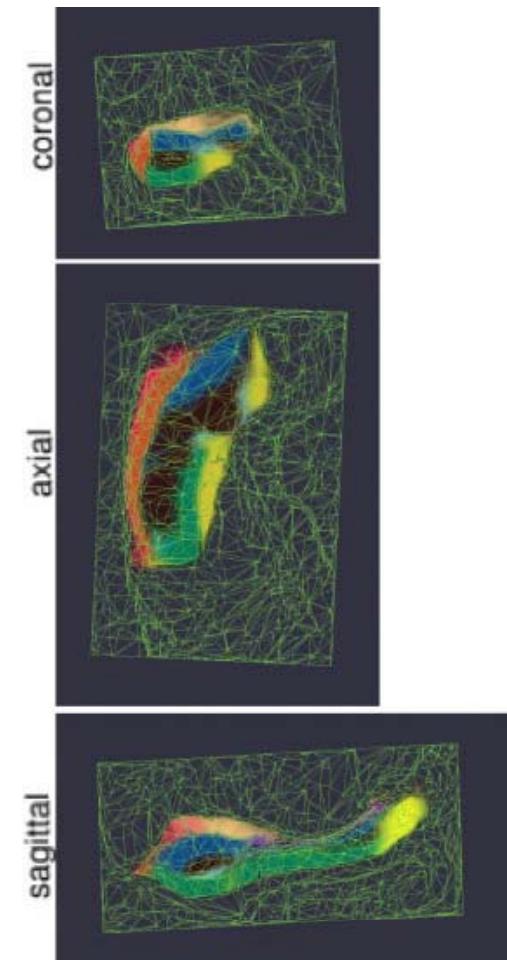
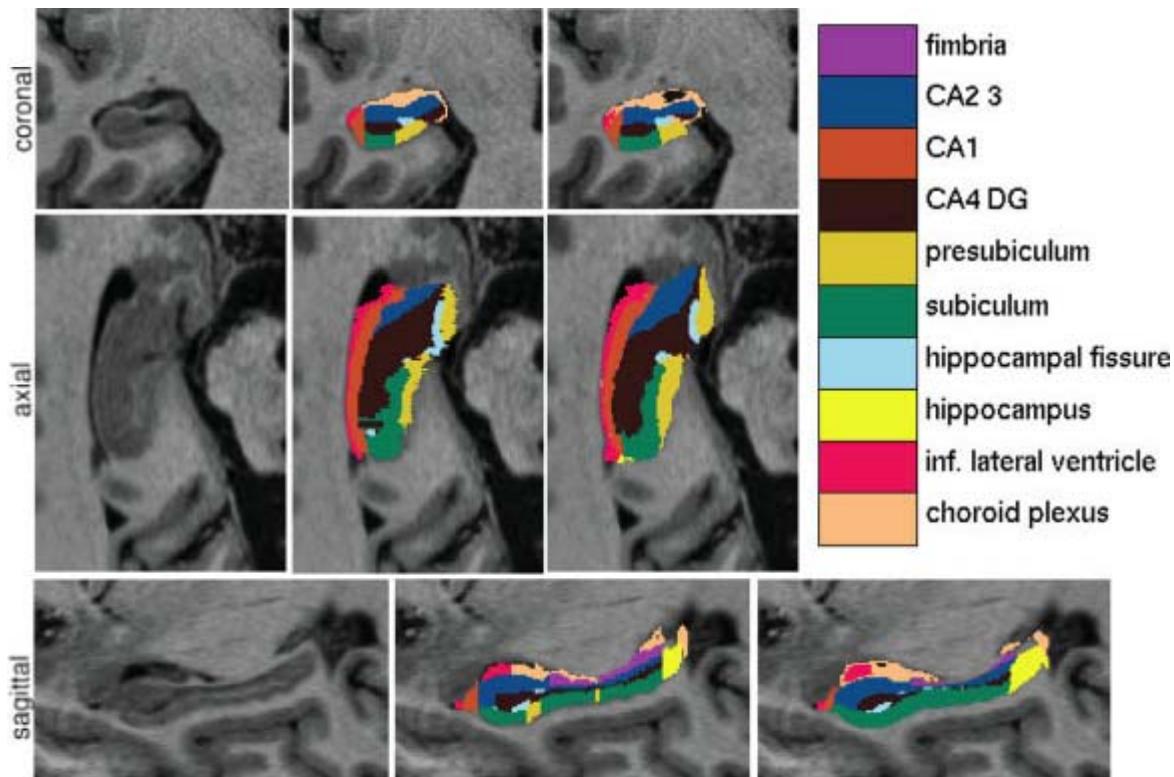
Improved ASL Perfusion Results



**zDFT =
zero-filled DFT**

By Dr. John Kornak, UCSF

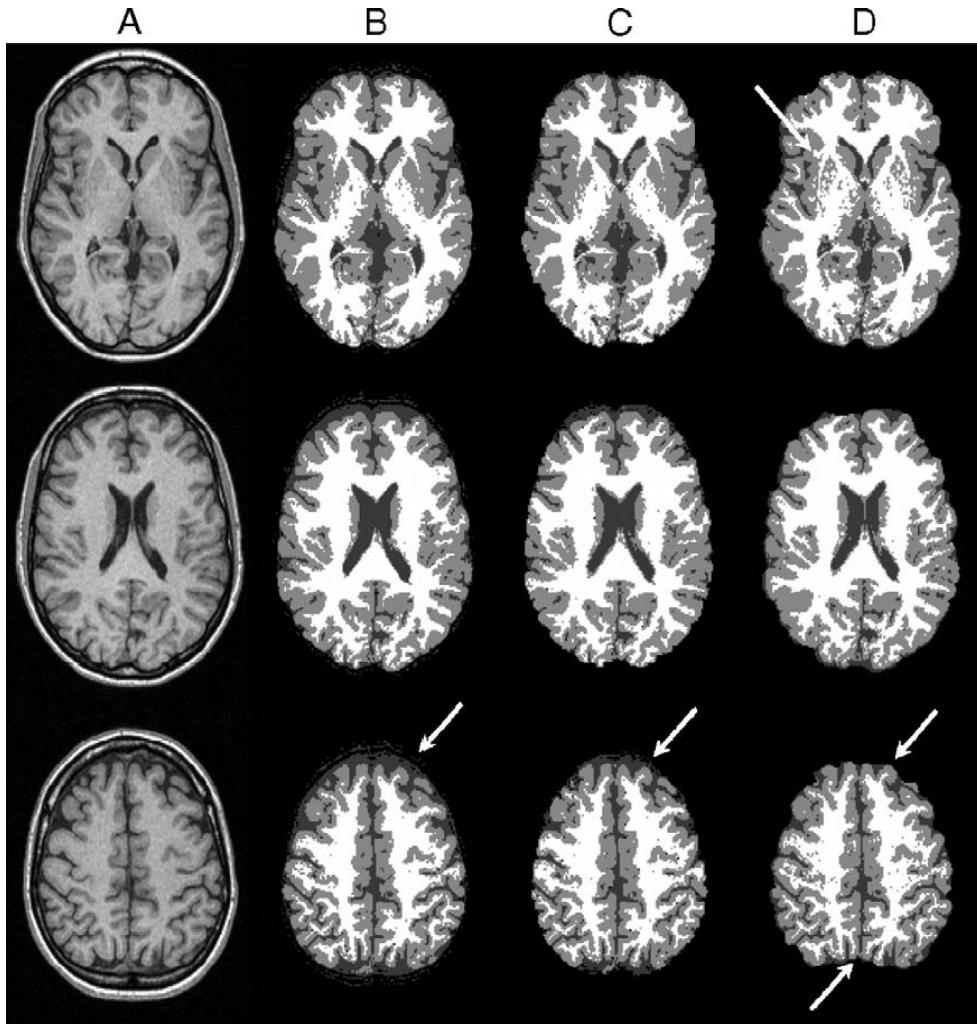
Bayesian Automated Image Segmentation



Bruce Fischl, MGH



Segmentation Using MLE

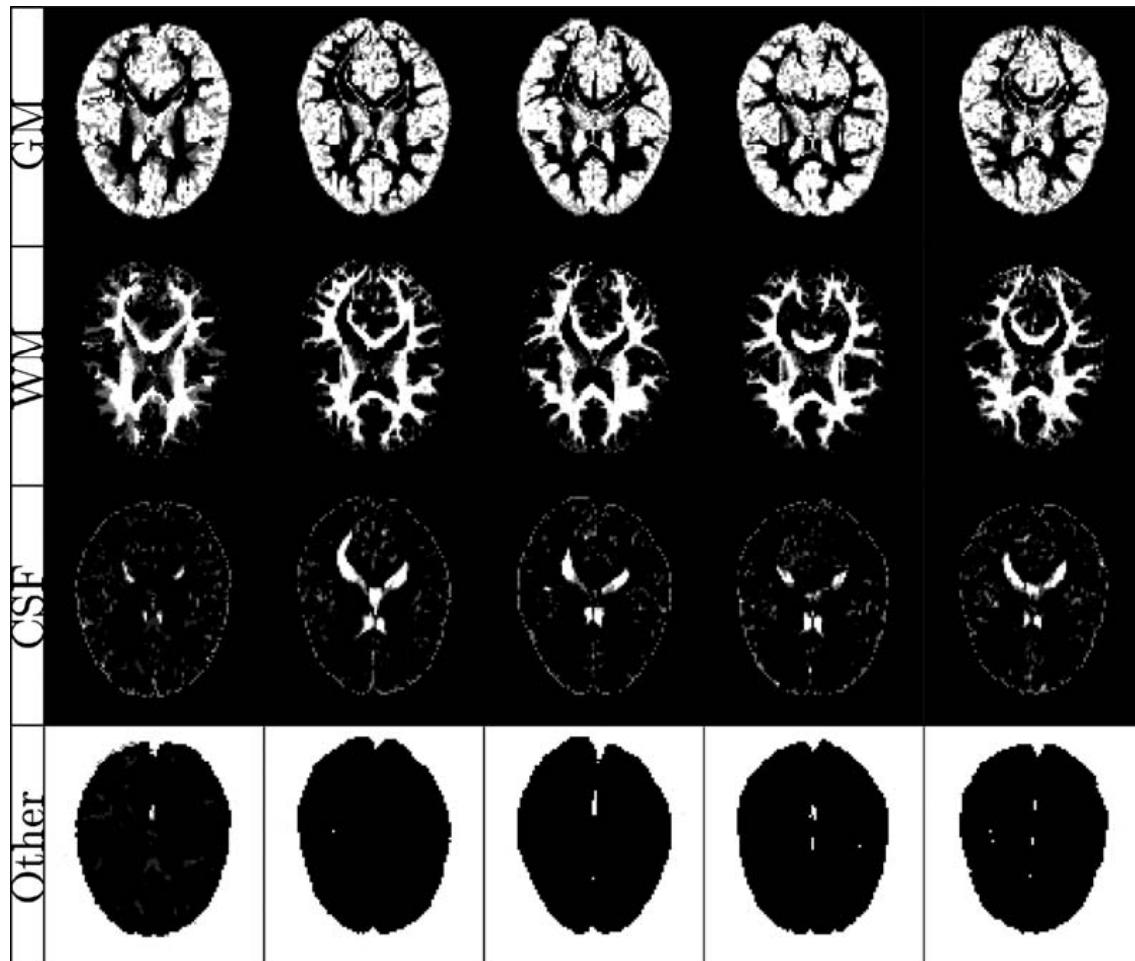


A: Raw MRI
B: SPM2
C: EMS
D: HBSA

from
Habib Zaidi, et al,
NeuroImage 32
(2006) 1591 – 1607

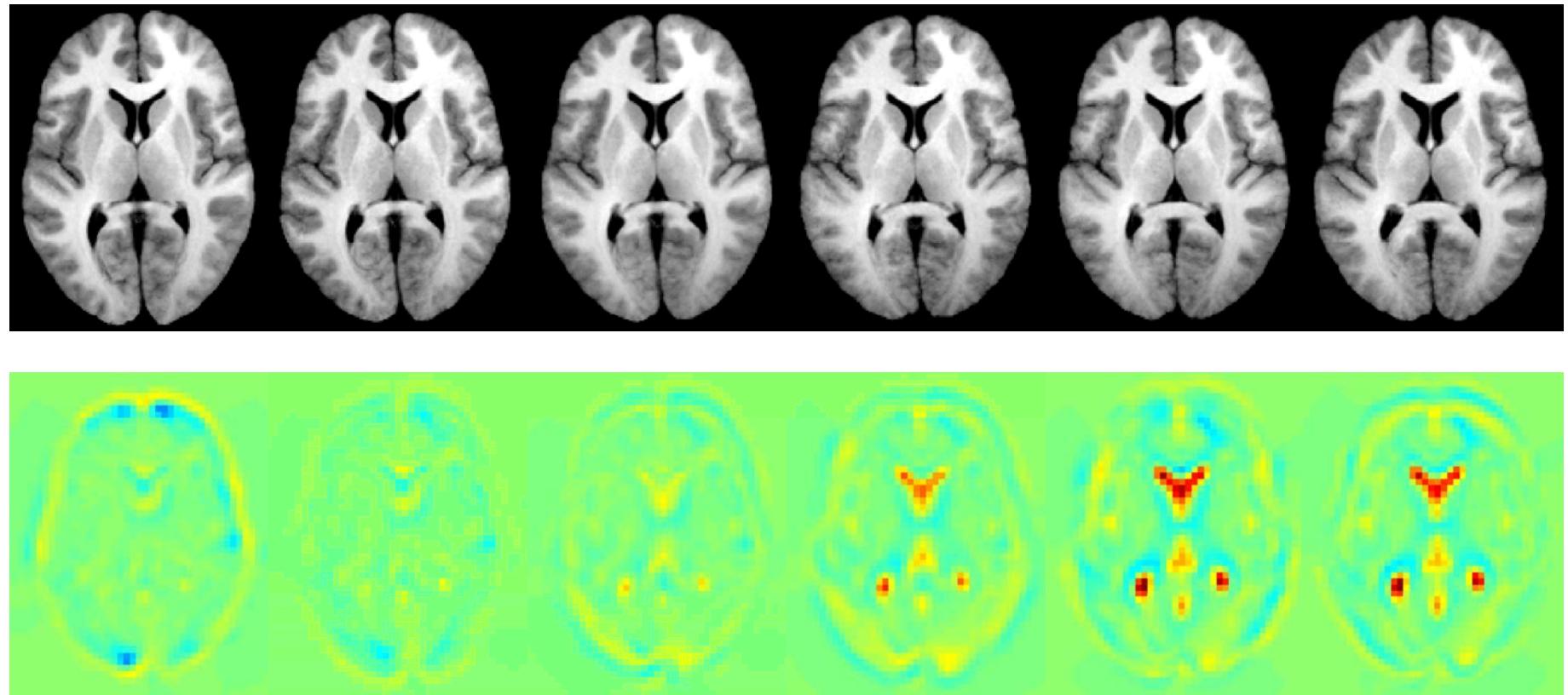


Population Atlases As Priors



Dr. Sarang Joshi, U Utah, Salt Lake City

Population Shape Regressions Based Age-Selective Priors



Age = 29

33

37

41

45

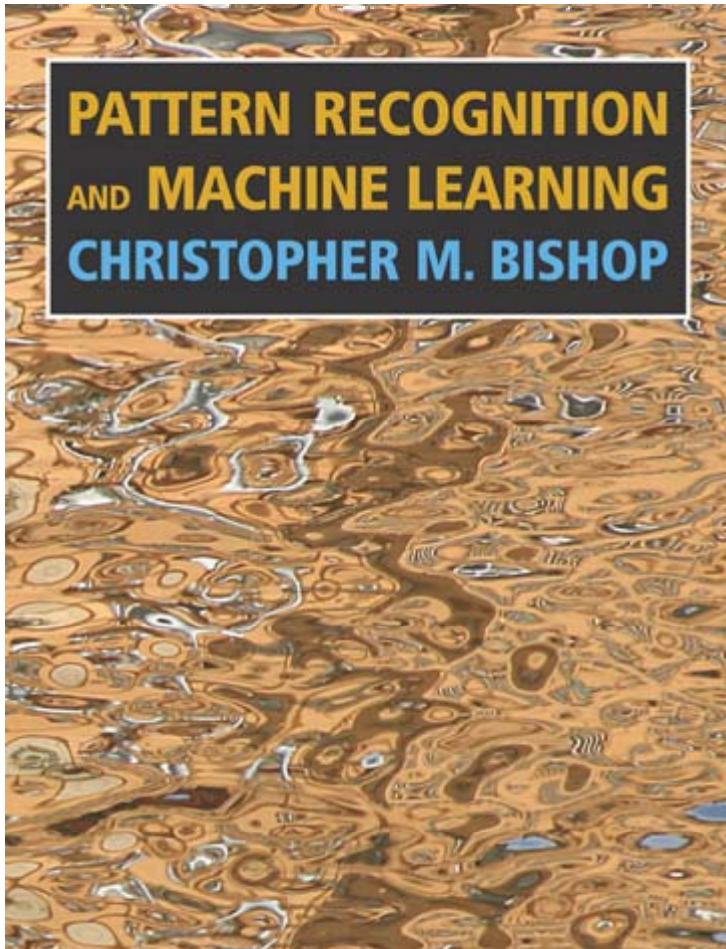
49

Dr. Sarang Joshi, U Utah, Salt Lake City

Imaging Software Using MLE And MAP

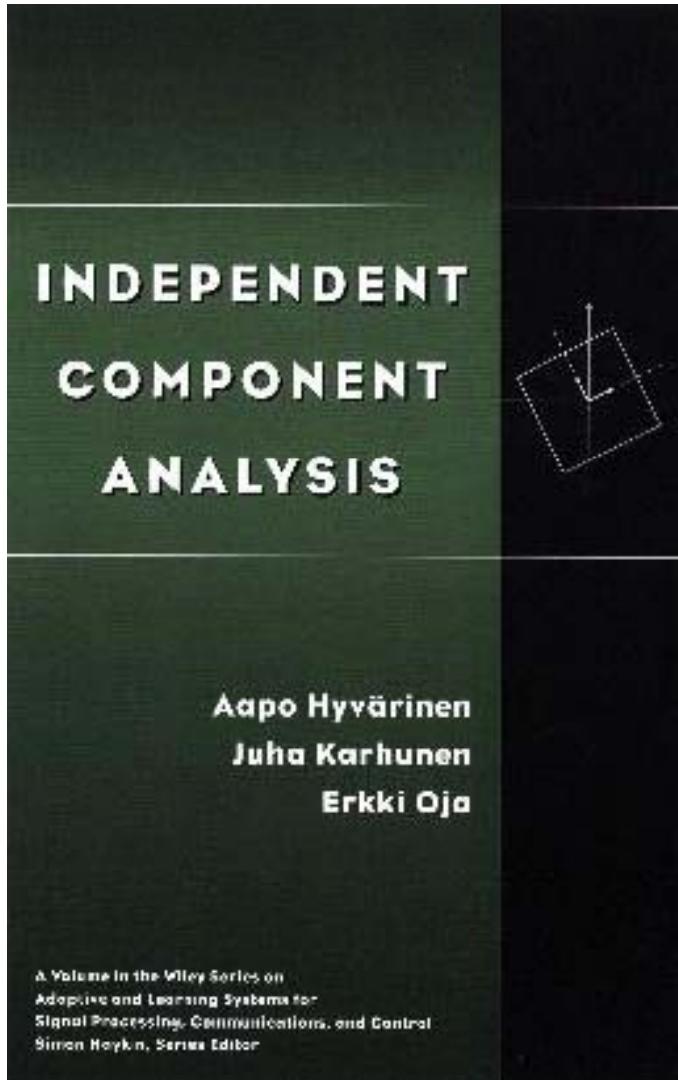
Packages	Applications	Languages
VoxBo	fMRI	C/C++/IDL
MEDx	sMRI, fMRI	C/C++/Tcl/Tk
SPM	fMRI, sMRI	matlab/C
iBrain		IDL
FSL	fMRI, sMRI, DTI	C/C++
fmristat	fMRI	matlab
BrainVoyager	sMRI	C/C++
BrainTools		C/C++
AFNI	fMRI, DTI	C/C++
Freesurfer	sMRI	C/C++
NiPy		Python

Literature



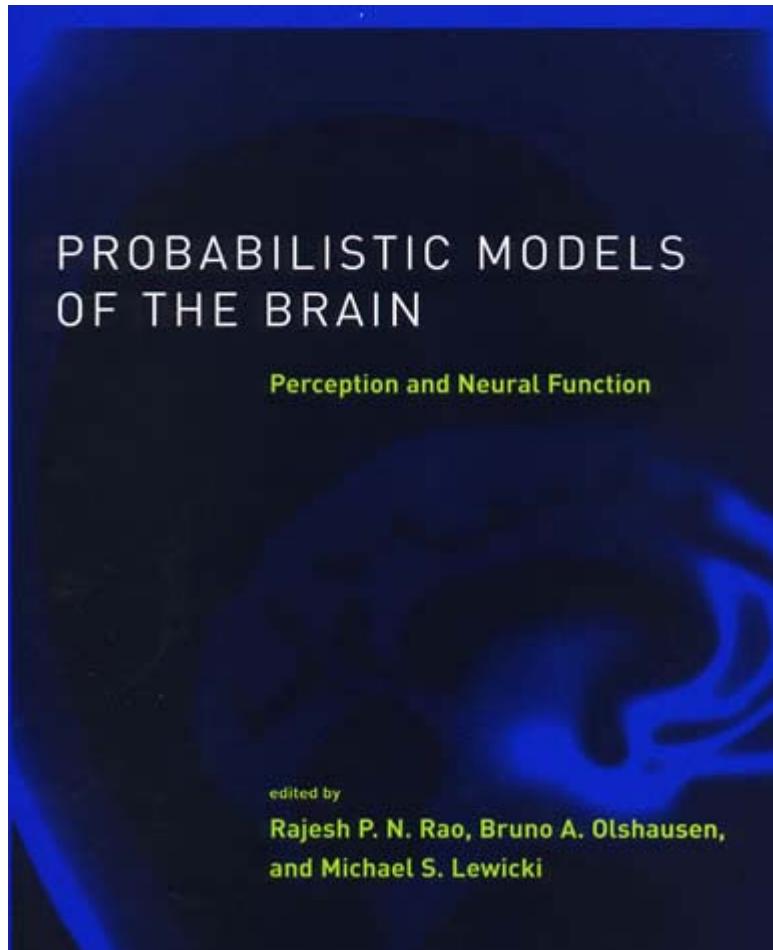
2 Probability Distributions	67
2.1 Binary Variables	68
2.1.1 The beta distribution	71
2.2 Multinomial Variables	74
2.2.1 The Dirichlet distribution	76
2.3 The Gaussian Distribution	78
2.3.1 Conditional Gaussian distributions	85
2.3.2 Marginal Gaussian distributions	88
2.3.3 Bayes' theorem for Gaussian variables	90
2.3.4 Maximum likelihood for the Gaussian	93
2.3.5 Sequential estimation	94
2.3.6 Bayesian inference for the Gaussian	97
2.3.7 Student's t-distribution	102
2.3.8 Periodic variables	105
2.3.9 Mixtures of Gaussians	110
2.4 The Exponential Family	113
2.4.1 Maximum likelihood and sufficient statistics	116
2.4.2 Conjugate priors	117
2.4.3 Noninformative priors	117
2.5 Nonparametric Methods	120
2.5.1 Kernel density estimators	122
2.5.2 Nearest-neighbour methods	124
Exercises	127
3 Linear Models for Regression	137
3.1 Linear Basis Function Models	138
3.1.1 Maximum likelihood and least squares	140
3.1.2 Geometry of least squares	143
3.1.3 Sequential learning	143
3.1.4 Regularized least squares	144
3.1.5 Multiple outputs	146
3.2 The Bias-Variance Decomposition	147
3.3 Bayesian Linear Regression	152
3.3.1 Parameter distribution	153
3.3.2 Predictive distribution	156
3.3.3 Equivalent kernel	157
3.4 Bayesian Model Comparison	161
3.5 The Evidence Approximation	165

Literature



- Estimation Theory 77
 - 4.1 Basic concepts 78
 - 4.2 Properties of estimators 80
 - 4.3 Method of moments 84
 - 4.4 Least-squares estimation 86
 - 4.4.1 Linear least-squares method 86
 - 4.4.2 Nonlinear and generalized least squares * 88
 - 4.5 Maximum likelihood method 90
 - 4.6 Bayesian estimation * 94
 - 4.6.1 Minimum mean-square error estimator 94
 - 4.6.2 Wiener filtering 96
 - 4.6.3 Maximum a posteriori (MAP) estimator 97
 - 4.7 Concluding remarks and references 99
- Problems 101
- 5 Information Theory 105
 - 5.1 Entropy 105
 - 5.1.1 Definition of entropy 105
 - 5.1.2 Entropy and coding length 107
 - 5.1.3 Differential entropy 108
 - 5.1.4 Entropy of a transformation 109
 - 5.2 Mutual information 110
 - 5.2.1 Definition using entropy 110
 - 5.2.2 Definition using Kullback-Leibler divergence 110

Literature



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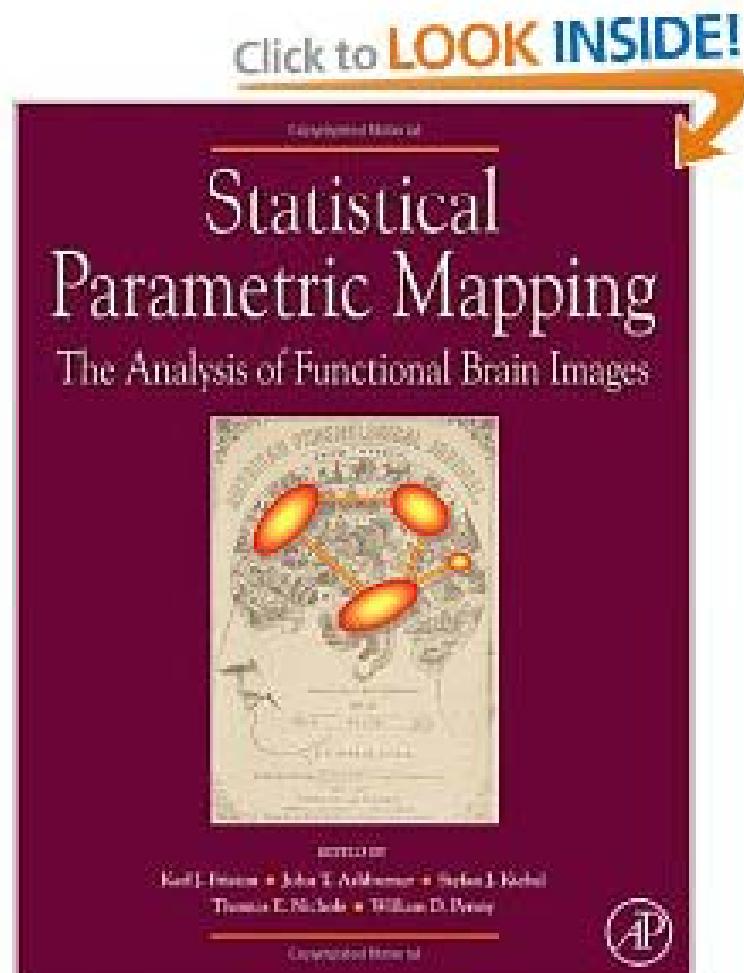
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